# EFFECT OF VORTEX GENERATOR ON BLOOD FLOW CHARACTERISTIC ON REAL PATIENT SPECIFIC DATA

# NURSYASYA AMANINA BINTI MOHD FIZAL

# UNIVERSITI TEKNIKAL MALAYSIA MELAKA

### EFFECT OF VORTEX GENERATOR ON BLOOD FLOW CHARACTERISTIC ON REAL PATIENT SPECIFIC DATA

# NURSYASYA AMANINA BINTI MOHD FIZAL

A report is submitted in fulfilment of the requirements for the degree of Bachelor of Mechanical Engineering with Honours

**Faculty of Mechanical Engineering** 

# UNIVERSITI TEKNIKAL MALAYSIA MELAKA

2020

# DECLARATION

I declare that this project "Effect of Vortex Generator on Blood Flow Characteristic on Real Patient Specific Data" is the result of my own work except as cited in the references.

Signature	:
Name	: Nursyasya Amanina Binti Mohd Fizal
Date	:

# APPROVAL

I hereby declare that I have read this project report and in my opinion this report is sufficient in terms of scope and quality for the award of the degree of Bachelor of Mechanical Engineering.

Signature	:
Name of Supervisor	:Dr. Mohamad Shukri Bin Zakaria
Date	:

### ABSTRACT

Blood clot coagulation is the main concerned for people who are using Bileaflet Mechanical Heart Valve to replace the ruptured valve. Different design of vortex generator can affect the blood flow at the vicinity of the mechanical heart valve and therefore the velocity, pressure drops and wall shear stress are needed to be investigated. The study only includes steady state condition during peak systole at the aorta. The blunt edges vortex generators (without the aorta) showed lower average velocity with value of 0.80 m/s compared with the sharp edges of vortex generator. The blunt edges of vortex generator also improved the pressure gradient of the blood flow and the result was found 3.64 mmHg compared to the previous study which shows pressure gradient of  $10.45 \pm 0.94$  mmHg. Meanwhile, the wall shear stress was found 10.24 Pa which shows some reduction compared with the sharp edges of vortex generator. A blunt edges of Co-rotating vortex generator is considered a good application as it reduce the flow separation at the vicinity of the leaflets as well helps in reducing the formation of thrombosis. However, to compare with the mechanical heart valve with aorta, the result with the aorta is less prone to blood clotting. A reduction with results of 2.3955 mmHg and 8.845 Pa in pressure drop and wall shear stress respectively indicates more delayed flow separation compared with the mechanical heart valve without aorta. This shows the simulation with the aorta needs to be included to investigate the reduction in blood clot.

### ABSTRAK

Pembekuan darah beku adalah kebimbangan utama bagi orang yang menggunakan Injap Jantung Mekanik Bileaflet untuk menggantikan injap yang rosak. Reka bentuk penjana pusaran yang berbeza boleh mempengaruhi aliran darah di sekitar injap jantung mekanikal dan oleh itu halaju, penurunan tekanan dan tekanan ricih dinding perlu diselidiki. Kajian ini hanya merangkumi keadaan stabil semasa puncak sistol di aorta. Penjana pusaran berbucu tumpul (tanpa aorta) menunjukkan halaju purata yang lebih rendah dengan nilai 0.80 m/s berbanding dengan penjana pusaran berbucu tajam. Bucu tumpul penjana pusaran juga meningkatkan kecerunan tekanan aliran darah dan hasilnya didapati 3.64 mmHg berbanding kajian sebelumnya yang menunjukkan kecerunan tekanan 10.45 ± 0.94 mmHg. Sementara itu, tegasan ricih dinding dijumpai 10.24 Pa yang menunjukkan sedikit pengurangan berbanding dengan penjana pusaran berbucu tajam. Bucu tumpul penjana pusaran yang berbentuk berpusing bersama dianggap sebagai aplikasi yang baik kerana ia mengurangkan pemisahan aliran di sekitar injap jantung dan juga membantu mengurangkan pembentukan trombosis. Namun, jika dibandingkan dengan injap jantung mekanikal dengan aorta, hasilnya dengan aorta kurang terdedah kepada pembekuan darah. Pengurangan dengan keputusan 2.3955 mmHg dan 8.845 Pa pada tekanan kecerunan dan ricih dinding menunjukkan pemisahan aliran yang lebih lambat berbanding dengan injap jantung mekanikal tanpa aorta. Ini menunjukkan simulasi dengan aorta perlu disertakan untuk menyiasat pengurangan pembekuan darah.

### ACKNOWLEDGEMENT

Praise to Allah S.W.T, the Almighty on whom ultimately we depend for substance and guidance and for the strengths and His blessing in completing this report.

Special appreciation goes to my supervisor, Dr. Mohamad Shukri Bin Zakaria, whose continuous guidance, constructive comments and useful advices was very valuable to me and have contributed to the success of this report Certainly, not to forget Faculty of Mechanical Engineering, UTeM for giving me the opportunity to do researches in order to complete my degree in Bachelor of Mechanical Engineering.

Sincere thanks to my friend, Edzzry Indrawan Bin Faizal Edzuan, Muhammad Nazhiim Bin Mohd Nazri, Yew Sin Wei, Nur Syahirah Binti Ahmad, Aina Nazira Binti Abdul Muttalib and Nur Batrisyia Husna Binti Zainurin for the support in helping me with my final year project. Not to forget other friends that support and encourage me continuously in completing my study.

Last but not least, my deepest gratitude goes to my beloved family for their endless love, support and encouragement especially to my parent; Mr. Mohd Fizal Bin Abd Dzubir and Mrs. Junaidah Binti Yusof. To those who indirectly contributed in this research, your kindness means a lot, thank you.

## **TABLE OF CONTENTS**

i

ii

iii

v

viii

xi

xii

xiii

xiv

# DECLARATION APPROVAL ABSTRACT ABSTRAK ACKNOWLEDGEMENTS TABLE OF CONTENTS LIST OF FIGURES LIST OF APPENDICES LIST OF TABLES LIST OF ABBREVIATIONS LIST OF SYMBOLS

# CHAPTER

1	INTRODUCTION	1
	1.1 Background of Study	1
	1.2 Problem Statement	4
	1.3 Objectives	5
	1.4 Scope of Study	5
	1.5 General Methodology	6
2	LITERATURE REVIEW	8
	2.1 Background of Human Body	8
	2.1.1 Blood Circulatory System	9
	2.1.2 Anatomical Structures of Aorta	11
	2.2 Modelling Blood Flow in Cardiovascular System	13
	2.2.1 Properties of Fluid Flow	14
	2.2.2 Model of Wall Aorta	15
	2.3 Mechanical Heart Valve	16
	2.4 Computational Fluid Dynamics	19
	2.4.1 Governing Equation	20
	2.5 Vortex Generator Applications	21

	2.5.1 Effect of Vortex Generator on Hatchback type of	21
	cars	24
	2.5.2 Effect of Vortex Generator on Swept Constant	24
	Chord Half-model	07
	2.5.3 Effect of Vortex Generator on Mechanical Heart	27
	Valve	
3	METHODOLOGY	30
	3.1 Introduction	30
	3.2 Software	32
	3.2.1 Mimics Medical 21.0	32
	3.2.2 SOLIDWORKS	33
	3.2.3 Geomagic Design X	36
	3.2.4 ANSYS	37
	3.3 CFD Simulation Process (MHV without Aorta)	37
	3.3.1 Pre-processing	37
	3.3.2 Solver Execution	41
	3.4 CFD Simulation Process (MHV with Aorta)	42
	3.4.1 Pre-processing	42
	3.4.2 Solver Execution	48
	3.5 Geometry of Vortex Generator	49
4	RESULTS AND DISCUSSION	50
	4.1 Results and Discussion of Mechanical Heart Valve	50
	without Aorta	
	4.1.1 Grid Independency Test	50
	4.1.2 Simulation Results	51
	4.1.3 Comparison of Flow Characteristics with Previous	54
	Study	
	4.2 Results and Discussion of Mechanical Heart Valve with Aorta	57

	4.2.1 Grid Independency Test	57
	4.2.2 Simulation Results	59
	4.2.3 Comparison of Flow Characteristics with MHV	64
	Results	
5	CONCLUSION AND RECOMMENDATIONS	67
	REFERENCES	69
	APPENDICES A	77
	APPENDICES B	78

# LIST OF FIGURES

TITLE

PAGE

FIGURE

1.1 (a)	Aortic valve stenosis	2
1.1 (b)	Aortic valve regurgitation	2
2.1	Blood Circulatory System	10
2.2	Anatomical structure of aorta	11
2.3	Position of MHV in the aorta	12
2.4	Overview of aorta structure in the human body	12
2.5	Network reconstruction of blood modelling by stages	13
2.6	Geometry of physiologic circulation	14
2.7	Pulsatile flow of physiologic circulation by using inlet	15
	velocity	
2.8	Model of rigid wall aorta	16
2.9	Types of heart valve prostheses	18
2.10 (a)	Velocity profile at the rear end car	22
2.10 (b)	Air flow around the VG	22
2.11	Pressure distribution over hatchback car	23
2.12	Velocity distribution over hatchback car	23
2.13	Swept Constant Chord Half-model schematic views	24
2.14	Surface streamlines of SCCH without VGs	25
2.15	Surface streamlines of SCCH with VGs	25
2.16	Pressure distribution of SCCH with and without VGs	26
2.17	Effect of VGs on lift performance	26
2.18	Velocity vectors and vorticity contours at four different	28
	phases during cardiac cycle with and without VGs	

2.19	RSS contour at four different phases with and without	29
	VGs	
3.1	Flowchart of methodology of the study	31
3.2	X-ray images of patient's heart	32
3.3	Image of aorta	33
3.4	3D CAD drawing of mechanical heart valve	34
3.5	3D CAD drawing of vortex generator	35
3.6	Location of VGs in mechanical heart valve	35
3.7	Assembled mechanical heart valve	36
3.8	Polyhedral meshing grid of mechanical heart valve	38
3.9	Details of generated mesh	38
3.10	Named selection for inlet	39
3.11	Named selection for outlet	40
3.12	Named selection for leaflet 1	40
3.13	Named selection for leaflet 2	40
3.14	Generated meshing of mechanical heart valve with aorta	43
3.15	Details of generated mesh	43
3.16	Named selection for inlet	44
3.17	Named selection for outlet 1	45
3.18	Named selection for outlet 2	45
3.19	Named selection for outlet 3	46
3.20	Named selection for outlet 4	46
3.21	Named selection for leaflet 1	47
3.22	Named selection for leaflet 2	47
3.23	Direction of blood flow through the leaflet	49
4.1	Grid Independency Test for mechanical heart valve	51
	without aorta	
4.2	Convergence result of mechanical heart valve	52
4.3	Velocity contour at the centre plane of the MHV	53
4.4	3D velocity streamlines of the MHV	53
4.5	Velocity vector of the MHV	54
4.6	Graph of Velocity vs. Z-Direction	55
4.7	Wall shear stress of MHV	56

4.8	Grid independency test with aorta	
4.9	Convergence result of mechanical heart valve with aorta	59
4.10	Velocity contour of mechanical heart valve attached	60
	with the aorta	
4.11	Velocity vector of mechanical heart valve attached with	61
	the aorta	
4.12	3D velocity streamlines of the mechanical heart valve	61
	with aorta	
4.13	Pressure contour	62
4.14 (a)	Wall shear stress contour	63
4.14 (b)	Wall shear stress from the left side	63
4.15	Highest WSS at outlet 1	63
4.16	Graph of Velocity versus Z-Direction of MHV with and	65
	without aorta	

х

# LIST OF APPENDICES

APPENDIX	TITLE	PAGE
A	Gantt chart for PSM 1	77
В	Gantt chart for PSM 2	78

# LIST OF TABLES

# TABLE

# TITLE

# PAGE

1	Properties of blood	14
2	Summary of hemodynamic data of MHV with and	28
	without VGs	
3	Dimensions of prosthetic heart valve and VGs.	34
4	Zone type of boundary conditions	41
5	Zone type of boundary conditions	48
6	Grid independency test for mechanical heart valve	51
7	Comparison of pressure gradient with previous study	55
8	Comparison of average wall shear stress with previous study	57
9	Grid Independency Test for mechanical heart valve with aorta	58
10	Comparison of hemodynamic parameter with and	64
	without aorta	

# LIST OF ABBREVIATIONS

BMHV	Bileaflet Mechanical Heart Valve
MHV	Mechanical Heart Valve
RSS	Reynolds Shear Stress
VG	Vortex generators
CFD	Computational Fluid Dynamics
WSS	Wall Shear Stress
СТ	Computerized Tomography
MRI	Magnetic Resonance Imaging
Re	Reynolds number
SCCH	Swept Constant Chord Half-model
PG	Pressure Gradient
CAD	Computer-Aided Design

# LIST OF SYMBOLS

- $\rho$  Density of fluid
- $g_i$  Body force in i-direction
- $\mu$  Dynamic viscosity of the fluid
- u velocity

### **CHAPTER 1**

### **INTRODUCTION**

### 1.1 Background of Study

Heart valve replacement surgery is a one kind of surgery that quit popular these days. This surgery involves patient that happen to have damaged heart valve due to some diseases, infections or accidents (Zakaria et al., 2017). If the heart valve disease is uncured, people can suffer from stroke, chest pain, or even die due to heart attack. Aortic valve stenosis is one of the heart valve diseases which causes the heart's aortic valve become narrow and soon can prevent the blood from flow through the aorta. A clear diagram of aortic valve stenosis is shown in Figure 1.1 (a). According to a research, about 400,000 people died due to cardiovascular disease which major on heart valve disease in between 1998 and 2004 in Germany (Bongert et al.,2008). In 2006, the heart valve surgery became popular for the local and demand on skilled heart surgeon increased (Bongert, M., Geller, M., Pennekamp, W., Roggenland, D., & Nicolas, V., 2008). Meanwhile, an estimated 2.9 to 5.8 million more adults in the U.S. experienced aortic valve disease in 2016 as the percentage of people having the heart valve disease increase at the age of 65 years old and above (Evans, F. & Vinod H. Thourani, 2018).

Other than stenosis, aortic valve regurgitation also contributes in heart valve failure. Regurgitation is a backflow of blood during diastole (phase when heart muscles relaxes), where the blood flow backwards from the aorta to the left ventricle (Armstrong, G. P., 2018). Based on American Heart Association (2016), this disease can occur mostly due to aging, infection at the heart tissue and high blood pressure. It can make a person become exhausted and make them feel breathless due to the low oxygen being pumped through the heart as there are leakage occurs at the aortic valve where the blood will flow backwards from the aorta to the left ventricles.



Figure 1.1 (a) Aortic valve stenosis (M. C. S, 2018). (b) Aortic valve regurgitation (M.C. S, 2017)

Due to the leakage, the aortic valve did not operate efficiently and can lead to heart failure. Figure 1.1 (b) shows how the aortic valve regurgitation can occur.

There are two types of prosthetic heart valve that can be used to treat the uncured heart valve, which are Mechanical Heart Valve (MHV) and Bio-prosthetic Heart Valve (BHV). Mechanical Heart Valve is made of pyrolytic carbon and is the most preferable prosthetic heart valve among the patients as it is last long and only need to undergo replacement surgery once in a life time (Zakaria et al., 2017). Meanwhile, Bio-prosthetic heart valve is made of animal tissues and only last long for several years as it will degenerate due to calcification. Therefore, another surgery needs to be done to replace the damaged valve with the new one which make this prosthetic heart valve less preferable compared to MHV. However, despite of being the most preferable prosthetic heart valve, there are few complications occur on having MHV such as thrombosis and bleeding.

Previous study found that blood clot complication is highly risk and can cause stroke or cause the valve to fail itself. If there is some vessel injury occurs at the valve, low dilution of the activated clotting factors due to low cardiac output will trigger the blood coagulation and this can occur based on different anatomical positions. Besides that, the hemodynamic flow characteristic varies with different anatomical positions. Other than that, no current or circulation of the blood flow at Bileaflet Mechanical Heart Valve (BMHV) hinges caused by the sharp geometries, can lead to thrombosis. In contrast, blunt edges at the vicinity of the vortex generator leads to low level of platelet damage (Zakaria et al., 2017).

Besides sharp geometries, thromboembolism and platelet activation are the most crucial complications of having this type of heart valve replacement surgery as it creates a high shear stress caused by the blood flow (Yun et al., 2014).

### **1.2 Problem Statement**

Bileaflet Mechanical Heart Valve (BMHV) is the most common design of MHV and said to be the best design during this century. However, this type of MHV cannot run from the fact of thrombosis complication that can occur in the vicinity of the leaflet due to abnormal flow (Zakaria et al., 2017). Besides that, according to Zakaria et al (2017), current design of Bileaflet MHV has a weakness as there is a gap between hinge and leaflet (150µm), where higher risk of blood clot will occur. In order to reduce the blood clot, patients need to take blood thinner known as warfarin everyday based on doctor's prescription. This could drastically affect the lifestyle of the patients for his future days and also can affect the child mortality for married women. Based on researches, the vorticity in the shear layers disperse directly soon after leave the leaflet surfaces where the fastest streamwise of the vorticity deteriorate. This phenomenon occurs during peak systole, when there is no vortex generator installed at the bileaflet heart valve (Hatoum & Dasi, 2018). Besides that, it is found that the Reynolds Shear Stress (RSS) magnitudes at the peak systole is higher when VGs are not installed compared to the absence of the VGs. In order to reduce the RSS and pressure drop, as well as the velocity of the blood flow, VGs need to be attached to the bileaflet of the valve as it leads to the slowing down of the separation of flow and reduce the unsteadiness of the free shear at the shear layers (Hatoum & Dasi, 2018). Other than that, even though VGs give big impact to reduction of RSS, pressure drop and velocity, different types of VGs will give different value and effect of those parameters. Therefore, a better geometry design of vortex generator by using the Computational Fluid Dynamic (CFD) analysis of the blood flow can help to reduce the aggregation of blood clot.

### **1.3 Objectives**

Bileaflet Mechanical Heart Valve (BMHV) is the most preferred prosthetic valve during this era, which is symmetrical and relatively non-turbulent in term of blood clot influence, compared to other MHV type. The most prospering material used for MHV is pyrolytic carbon as it suits the condition of the body in term of biocompatibility (Helmus, M., & Cunanan, C., 2011). This project is cognate with the geometry design of the vortex generator and the effect on the blood flow which is rigorously scrutinises the blood clot issue. There are few objectives of this study in order to achieve a better result, which are as follows;

- 1) To develop CFD models of blood flow in vivo at the aortic valve.
- To improve the current vortex generator design by comparing with previous experimental studies.
- 3) To analyze the blood flow characteristics such as velocity, pressure drop and wall shear stress by using improved design of vortex generator attached to the real aorta.

### 1.4 Scope of Study

This study is focusing primarily on the effect of vortex generator on blood flow characteristic on real patient specific data. Type of prosthetic valve used in this study is Bileaflet Mechanical Heart Valve (BMHV) that resembling St. Jude Medical Regent Bileaflet Valve as it is the most thriving prosthetic valve for the heart valve replacement surgery based on the past research that gives better result compared to other type of prosthetic heart valve. Besides that, this study is also focusing on designing a new geometry of vortex generator in order to reduce the coagulation of the blood clot. Other than that, in this study, only the opening sequence of the leaflet will be covered. However, the effect of angle opening of the vortex generator will not be covered in this study.

### **General Methodology**

In order to achieve the objectives and scopes of this study, there are few actions need to be carried out in a correct sequence as follows:

1) Literature review.

Scholarly article, journal and past research thesis will be reviewed and summarized to help with the research.

2) Mimics software.

Mimics/Slicer software will be used to create medical imaging of the real patient's data.

3) SolidWorks software.

This software will be used to draw the mechanical heart valve with vortex generator.

4) Geomagic X software.

This software will be used to attach the mechanical heart valve and the medical imaging of the real patient's data.

5) Simulation.

Simulation of Computational Fluid Dynamics (CFD) models of blood flow in vivo at the aortic valve with vortex generator is simulated by using ANSYS.

6) Analysis and proposed solution.

Analysis of the blood flow characteristics due to blood clot with the presence of vortex generator will be done in terms of wall shear stress (WSS).